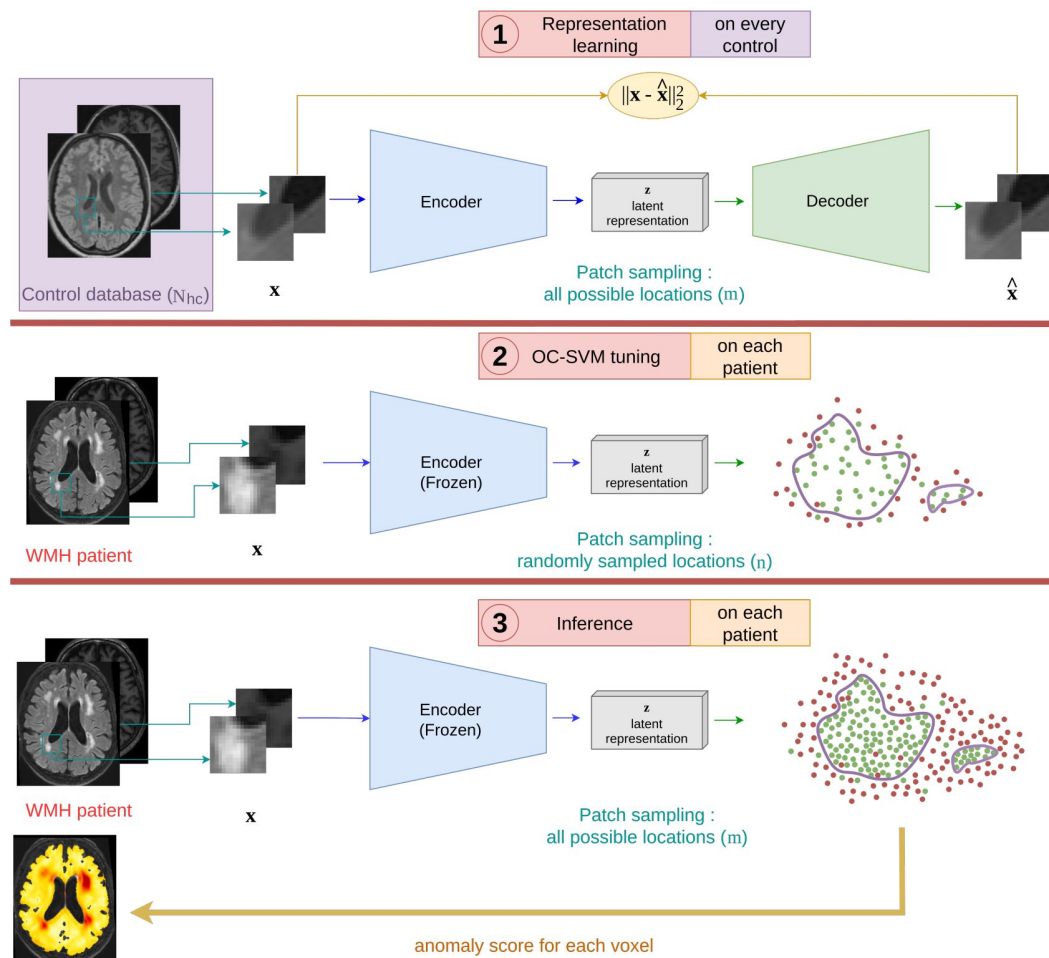


Introduction

- Unsupervised brain anomaly detection (UAD) methods have been proposed as an alternative to supervised models when the studied pathology is **rare** or when gathering fine expert **annotations** is too **challenging**.
- In this work, we propose a novel UAD method, with patient-specific characteristics, tailored to the task of lesion detection in multi-modal neuroimaging.

Unsupervised Anomaly Detection pipeline



1. Representation learning

A siamese auto-encoder [3] is trained on **control** (healthy) patches x only. Every possible location in the brain is sampled, thus constructing a structured latent space based on a L_{SAE} loss function combining a standard MSE in the image space and cosine similarity in the latent space.

$$L_{SAE}(x_1, x_2) = \sum_{t=1}^2 \|x_t - \hat{x}_t\|_2^2 - \alpha \cdot \cos(z_1, z_2)$$

2. One-Class SVM tuning

For each **patient** (pathological), a subset of available patches is sampled, their latent representation extracted, and a One-Class SVM [2] trained to estimate the support of the normative latent density distribution.

3. Inference

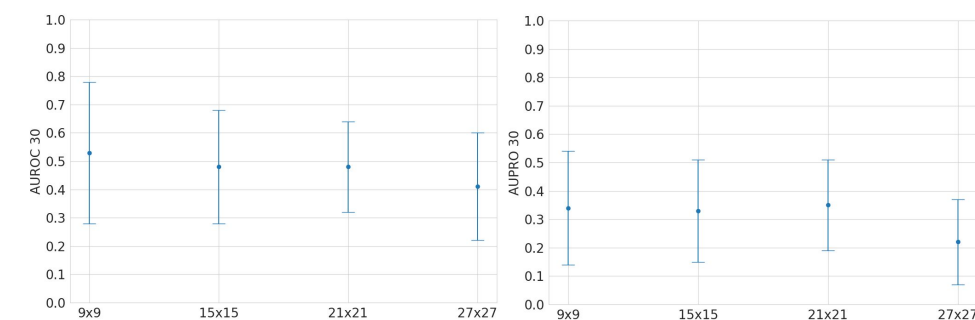
For each **patient**, latent representations of all patches are extracted and their distance to the boundary estimated. This will produce an anomaly score for each patch, that will be attributed to its central voxel to get the final anomaly map.

Experiments and Evaluation

- Control private dataset** : 75 paired T1w and FLAIR MRI on 1.5T Siemens Sonata scanner.
- Patient pubic dataset (WMH Challenge dataset)** : 60 paired T1w and FLAIR on 3 different hospitals with 3 scanners of different manufacturers, with associated 3D lesion mask.
- Performances of our UAD model are compared to the **two best performing UAD models** [4] [5] on the WMH challenge dataset. We also compare to our previous model [3] where latent representations extracted from the control dataset are used to tune one OC-SVM per voxel.
- Performances are evaluated based on **AU ROC**, **AU PRC** and best achievable **Dice** metrics. We also investigate **AU PRO** [6] which acts as an AU ROC normalised by the size of the lesion (highlight good detection of small lesions). AU ROC and AU PRO are also studied by limiting the false positive rate to **30%**, above which the anomaly maps can be considered degenerated.

Results and Discussion

- On overall, **performances of our UAD model are higher than all three other methods for all the metrics.**
- The **patient-specific tuning** with one OC-SVM per patient performs better than with multiple OC-SVM (one per localisation) as in [3].
- Automatically masking the cerebrospinal fluid from the score maps ('CSF Seg' in the table above) improves performances due to a reduction of false positives.
- Comparative study by hospital reveals a high variance of performances, possibly due to the difference of manufacturer with the training dataset.
- Performance of our model seems robust to change of patch size.



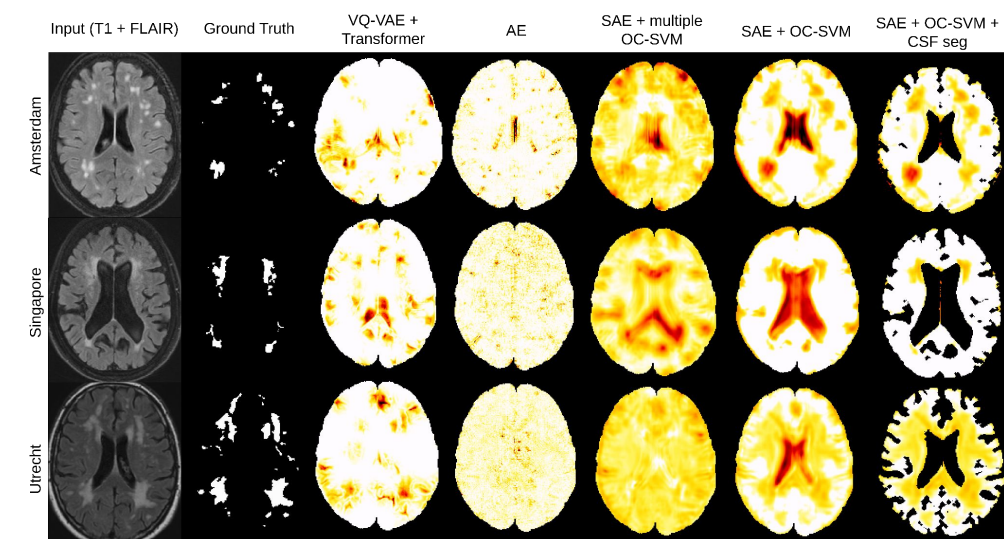
Influence of patch size on AU ROC 30 and AU PRO 30

3 hospitals	VQ-VAE + Transformer (Pinaya)	AE (Baur)	SAE + multiple OC-SVM (Alaverdyan)	SAE + OC-SVM (Ours)	SAE + OC-SVM + CSF seg (Ours)
AU ROC	0.69 ± 0.13	0.53 ± 0.09	0.52 ± 0.19	0.80 ± 0.09	0.81 ± 0.10
AU ROC 30	0.40 ± 0.20	0.20 ± 0.12	0.19 ± 0.16	0.48 ± 0.20	0.59 ± 0.17
AU PRC	0.065 ± 0.079	0.028 ± 0.030	0.023 ± 0.031	0.084 ± 0.099	0.165 ± 0.168
AU PRO	0.55 ± 0.10	0.50 ± 0.08	0.43 ± 0.17	0.71 ± 0.11	0.80 ± 0.07
AU PRO 30	0.19 ± 0.13	0.15 ± 0.07	0.09 ± 0.13	0.33 ± 0.18	0.48 ± 0.13
[Dice]	0.11 ± 0.10	0.06 ± 0.05	0.05 ± 0.05	0.14 ± 0.13	0.22 ± 0.17

Mean metric on every patient from the 3 different hospitals for each method. In bold are shown the best model and those for which Dunn's test with the best model returns a p -value > 0.01 .

Conclusion and future work

- Performance gap is observed between the reported performances by [4] and [5] and our reimplementation, this could be caused by the huge pre-training done in [5] on 15 000 FLAIR volumes, and by their limitation to the 4 central slices of the volume. [4] and [5] work with FLAIR only, and implement data augmentation processes that may fill the domain adaptation gap.
- In comparison with [3], we report that the OC-SVM patient-specific training strategy seems to improve the performances on this task.
- Future work includes implementing domain adaptation strategies to account for the diversity of the scanners used, testing on other datasets and work with 3D patches.



Exemple performance of the different methods on one example from each of the 3 hospitals

- [1] Muñoz-Ramírez V., Pinon, N., Forbes F., Lartizien C., Dojat, M.: "Patch vs. global image-based unsupervised anomaly detection in MR brain scans of early Parkinsonian patients". Machine Learning in Clinical Neuroimaging: 4th International Workshop, MLCN 2021.
- [2] Schölkopf B., Williamson R., Smola A., Shawe-Taylor J., Platt J.: "Support Vector Method for Novelty Detection." Advances in Neural Information Processing Systems 1999.
- [3] Alaverdyan, Z., Jung, J., Bouet, R., Lartizien, C.: "Regularized siamese neural network for unsupervised outlier detection on brain multiparametric magnetic resonance imaging: Application to epilepsy lesion screening". Medical Image Analysis 2020.
- [4] Baur C., Denner S., Wiestler B., Navab N., Albarqouni S.: Autoencoders for unsupervised anomaly segmentation in brain MR images: A comparative study. Medical Image Analysis 2021.
- [5] Pinaya W.H.L., Tudosiu P.-D., Gray R., Rees G., Nachev P., Ourselin S., Cardoso M. J.: Unsupervised brain imaging 3d anomaly detection and segmentation with transformers. Medical Image Analysis 2022
- [6] Bergmann P., Kilian P., Michael F., David S., Carsten S.: The MVTEC Anomaly Detection Dataset: A Comprehensive Real-World Dataset for Unsupervised Anomaly Detection.

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